## **MICROFLUIDIC PLATFORM FOR CULTURE AND LIVE CELL IMAGING OF CELLULAR MICROARRAYS JOHN BYCE, ALEX JOHNSON, SARAH REICHERT, ANTHONY SPRANGERS CLIENT:** RANDOLPH ASHTON, PH.D. **ADVISOR:** JOHN PUCCINELLI, PH.D. THE UNIVERSITY **DEPARTMENT OF BIOMEDICAL ENGINEERING, UNIVERSITY OF WISCONSIN – MADISON**



# ABSTRACT

Dopamine (DA) is a neurotransmitter that controls motor movement. When the neurons that release DA are deficient, patients become afflicted with Parkinson's disease (PD)<sup>[1]</sup>. Current therapies for PD lessen symptoms by supplementing the lost dopamine; this improves patient quality of life but does not treat the underlying disease mechanisms<sup>[2]</sup>. Neural stem cells (NSCs) have the potential to regenerate lost DA neurons and restore healthy dopamine levels in PD patients due to their ability to differentiate into all types of neurons <sup>[3]</sup>. Differentiation of NSCs is primarily regulated by the cellular microenvironment, which is in part determined by the localization and concentration of certain growth factors and other soluble molecules<sup>[4]</sup>. Microfluidic devices are advantageous for examining cell responses because they allow for highthroughput analysis with reduced costs, efficient manipulation of fluids, and certain fluid characteristics, such as laminar flow<sup>[5]</sup>. We adapted and fabricated a microfluidic device, originally devised by Jeon et al., that uses seven Christmas tree structures to generate concentration gradients of soluble molecules<sup>[6]</sup>. By integrating this system to flow gradients over a cellular microarray, the effects of various factors on NSC differentiation can be tested in a high-throughput manner. This will enable efficient identification of mechanisms related to DA neural differentiation and ultimately produce a homogenous population of neurons for regenerative medicine.

# INTRODUCTION

## MOTIVATION

- Neurodegenerative diseases result from loss of neuron structure and function
- Typically, mature neurons have limited proliferation capacity<sup>[3]</sup>
- Parkinson's disease: loss of dopaminergic neurons for movement control<sup>[1]</sup> ~ Prevalence: 500,000 individuals in the United States<sup>[1]</sup>
- Current therapies treat symptoms, not underlying cause<sup>[2]</sup>
  - Research suggests neural stem cells can generate all neuron types<sup>[3]</sup> ~ Knowledge of factors required to promote differentiation into specific neurons could lead to production of cells to replace damaged or dead neurons<sup>[3]</sup>



Forebrain

**Figure 1:** Primary Cause of Parkinson's Disease<sup>[7]</sup>. **A:** Parkinson's disease results from a loss of function in the dopaminergic neurons of the substantia nigra, located in the hindbrain. **B:** These neurons lose the ability to release dopamine, resulting in the symptoms commonly seen with Parkinson's disease.

Figure 2: Stem Cell-based Regenerative Medicine<sup>[8]</sup>. Neural stem cells can differentiate into all types of neurons. Differentiation is partially dependent on the localization and concentration of growth factors present in the cellular microenvironment. FGF: fibroblast growth factor. Shh: sonic hedgehog.

## BACKGROUND

## Advantages of microfluidics<sup>[5]</sup>

- Generate accurate gradients *in vitro*
- Minimize reagent volumes
- Allow for high resolution and sensitivity
- Permit laminar flow and low shear stress
- Facilitate high-throughput analysis
- Temporal gradient investigation<sup>[9]</sup>
- Gradients form during embryonic development
- Stem cell fates are directed by varying concentrations of soluble molecules
- Clonal microarrays<sup>[10]</sup>
- Cytophilic islands patterned on goldcoated glass
- Enable high-throughput screening
- establishing different colonies

Cytophili islands



Figure 3: Cellular Microarray<sup>[10]</sup>. Cells can be patterned on glass in a defined arrangement, making microarrays beneficial for high-throughput biological assays.





~ Islands separated by cytophobic regions ~ Cells seeded on device at clonal densities • Need a high-throughput method for

> Cytophobic region

- Integrate cellular microarray and microfluidic platform
- Generate concentration gradient
- Fick's law adequate diffusive mixing<sup>[11]</sup>:  $(\mathbf{v} \cdot \nabla C) = D \nabla^2 C$  $\sim$  Maximum allowable input flow rate: 1.0275 µL/min
- Low fluid shear stress on cells<sup>[12]</sup>:  $\tau_{max} = 12\mu Q/h^3$ ~ Maximum shear stress generated by device:  $0.021 \text{ dynes/cm}^2$ Support flow in multiple regimes
- Peclet's number convection vs. diffusion<sup>[13]</sup>: Pe = vh/D~ Convection dominates diffusion for *Pe* >> 1
- Peclet's number/Damkohler number convection vs. reaction<sup>[13]</sup>:  $Pe/Da = v/k_{on}R_s$ ~ Convection dominates reaction for Pe/Da >> 1

		VARIA
V	Velocity vector	
С	Concentration	
D	Diffusivity	
$ au_{max}$	Maximum shear stress per cell	
μ	Viscosity	
Soluble factors Microfluidic device		

Figure 5: Determining Cellular Response. By using our device to generate concentration gradients of various soluble factors, we hope to be able to

determine the influence of these factors on neural stem cell differentiation.

## Christmas Tree Microfluidic Design<sup>[6]</sup>





Microscope stage

Figure 7: Microfluidic Platform Integration

Imaging of the device is possible due to an opening in the microscope stage where it can placed and viewed with an objective from underneath. The PDMS component is oxidized to a glass bottom piece, but they are separated in the figure for ease of viewing. This glass has a section removed to allow for integration of the gold-coated glass piece that contains the cellular microarray. The microarray will be affixed to the PDMS prior to imaging and removed afterwards to allow for further experimentation with the cells.

# **DESIGN CRITERIA**





# FINAL DESIGN

## SIMULATION

• COMSOL: finite element analysis software • Simulated design functionality



Figure 8: COMSOL Analysis. Concentrations of 0  $\mu$ M and 25  $\mu$ M were input into the two inlets of one Christmas tree structure. Creep flow was used to simulate the flow of fluids through the channels. The resulting concentrations in the cell channels are shown above.

 Quantitatively compared results from COMSOL analysis and experimental device

- Determined accuracy of experimental device
- COMSOL parameters
- Flow rate: 1µL/min
- Inlet 1 concentration: 25 μM
- Inlet 2 concentration: 0 μM
- Experimental device parameters • Flow rate: 1 μL/min
- Inlet 1 concentration: 25 μM
- Inlet 2 concentration: 0 μM
- Compared concentrations in each channel (normalized to maximum concentrations)

- Integrate microarray
- Confirm adequate seal is formed
- Confirm removal without damage

- parkinsons\_disease\_backgrounder.htm

- 11. Ficks: S. Bird, Transport Phenomena Revised Second Edition: John Wiley & Sons, 2007.



# RESULTS



## EXPERIMENTAL

Gradient generated in experimental device

## 4x magnificatio **Figure 11: Experimental Device Performance Verification.** Fluorescence testing with 25 $\mu$ M dextran-fluorescein

isothiocyanate (FITC) and ultra-filtered deionized water (0  $\mu$ M) input into the inlet ports at a rate of  $1 \mu L/min$ .

## COMPARISON



Figure 12: Comparison of COMSOL Analysis and **Experimental Device Performance.** Solutions of 25 µM dextran-FITC and ultra-filtered deionized water (0  $\mu$ M) were input into the two inlet ports at a flow rate of 1  $\mu$ L/min. Fluorescence was measured at three locations in

each of the cell channels and averages were compared to the expected results based on COMSOL analysis.

# **FUTURE WORK**

- Incorporate cells
- Ensure viability
- Determine response to factors

# **ACKNOWLEDGEMENTS**

Dr. John Puccinelli, Dr. Randolph Ashton, Dave Buschke, John Guckenberger, Brian Freeman, Greg Czaplewski, Tracy Drier

# REFERENCES

- 1. NINDS. (2011, 12 October). National Institute of Neurological Disorders and Stroke Parkinson's Disease Backgrounder. Available: http://www.ninds.nih.gov/disorders/parkinsons\_disease/
- 2. University of California, San Francisco. (2011, 8 December). Biology of Neurodegeneration. Available: http://ind.ucsf.edu/causetocure/biology 3. NINDS. (2011, 8 December). National Institute of Neurological Disorders and Stroke – The Life and Death of a Neuron. Available: http://www.ninds.nih.gov/disorders/brain\_basics/ninds\_neuron.htm
- 4. D. E. Discher, *et al.*, "Growth factors, matrices, and forces combine and control stem cells," Science, vol. 324, p. 1673, 2009. 5. G. M. Whitesides. "The origins and the future of microfluidics," *Nature*, vol. 442, no. 27, pp. 368-373, Jul. 2006 6. N. L. Jeon, *et al.*, "Generation of solution and surface gradients using microfluidic systems," *Langmuir*, vol. 16, pp. 8311-8316, 2000.
- 7. A. Naik. (2011, 6 November). Parkinson's Disease. Available: http://drarunlnaik.com/parkinsons\_disease 8. T. Petros, et al., "Pluripotent stem cells for the study of CNS development," *Frontiers in Molecular Neuroscience*, vol. 4, p. 1-12.
- 9. G. Lupo, et al., "Mechanisms of Ventral Patterning in the Vertebrate Nervous System," Nat Rev Neurosci, vol. 7, pp. 103-114, 2006 10. R. S. Ashton, et al., "High Throughput Screening of Gene Function in Stem Cells Using Clonal Microarrays," Stem Cells, vol. 25, pp. 2928-2935, 2007.
- 12. Shear: L. Kim, et al., "Microfluidic arrays for logarithmically perfused embryonic stem cell culture," Lab Chip, vol. 6, pp. 394-406, 2006. 13. L. N. Przybyla, J. Voldman, "Attenuation of extrinsic signaling reveals the importance of matrix remodeling on maintenance of embryonic stem cell self-renewal," *Developmental Biology*, vol. 109, pp. 835-840, 2012.