

MOTIVATION

- Facilitate oncologist researches in quantifying thermal insulation of samples of rodent skin
- Currently, there two methods available to researchers that are not accurate and/or costly:
- Infrared thermometer of thermal imaging camera (Figure 1)
- Thermtest MP-1 device (Figure 2)



Figure 1: Commercially available Omega infrared thermometer [1].

Problem Statement

• There is not a cost effective, accurate device to measure the thermal conductance of rodent skin samples as required for oncology research.

BACKGROUND

- Skin is a complex system in its anatomy and physiological function, including heat regulation through dissipation.
 - Adipose tissue stores thermal energy close to the skin surface [3].
 - Lamellar bodies carry cargo necessary for maintaining homeostatic temperature [4].
- Heat transfer is closely related to metabolism, the net sum of reactions that provide the body with energy and consume it.
- Increased heat dissipation through less insulative skin can increase metabolic rate [5].
- Evaporative cooling causes inaccuracies in non-contact temperature measurement
 - Water in skin is heated and evaporates, releasing thermal energy.
 - Direct contact with skin prevents this evaporation from occurring.

DESIGN CRITERIA

- The device must:
- Heat skin sample with $34^{\circ}C \pm 0.5^{\circ}C$ pulses
- Accurately measure temperature within 0.1°C
- Accommodate samples of ex-vivo rodent skin 4x2 cm and 50-100 µm thick

Stratum corneum — Granular layer-Spinous layer ----Basal layer -

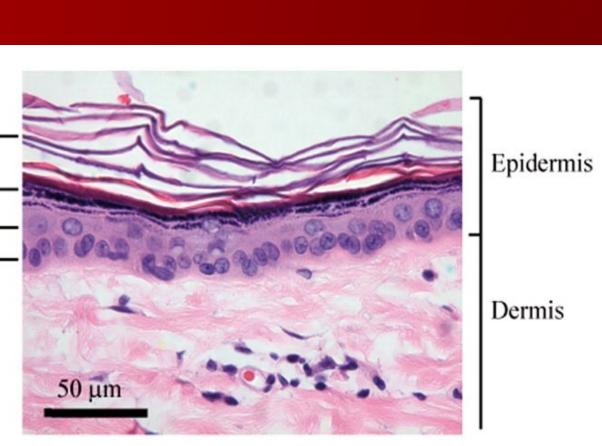


Figure 3: Side cut microscopy of the layering in skin [4].

Figure 4: Illustration of evaporative cooling [6]

- Measure heat transfer without being influenced by evaporative cooling
- Display temperature data graphically in relation to time
- Avoid damage to skin samples and withstand intended use



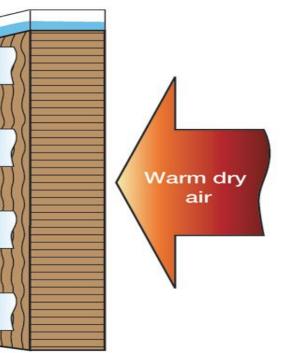
Analysis of Insulating Properties of Skin (Rodent)

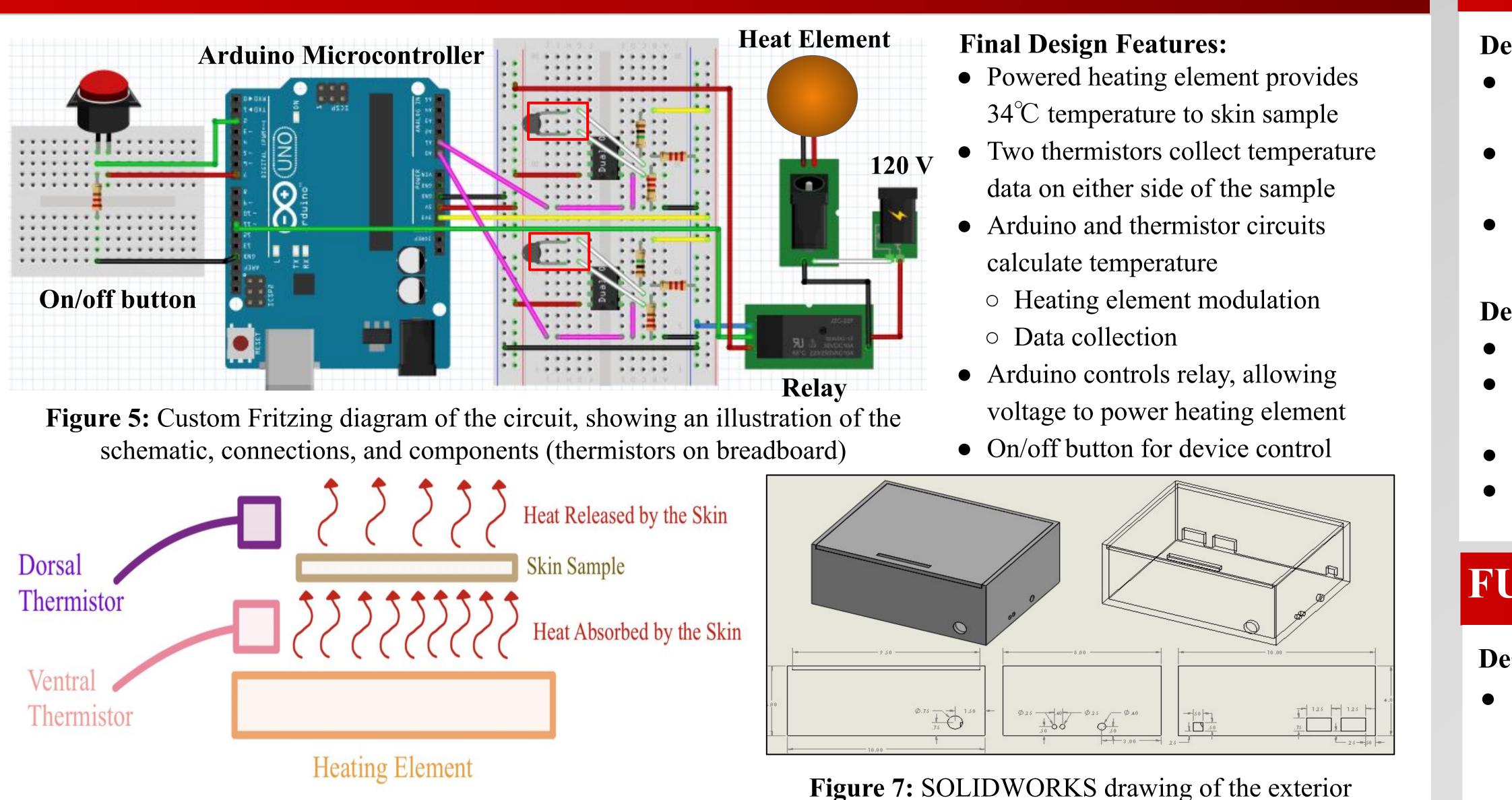
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FINAL DESIGN



Figure 2: Thermtest MP-1 device measurement platform [2].





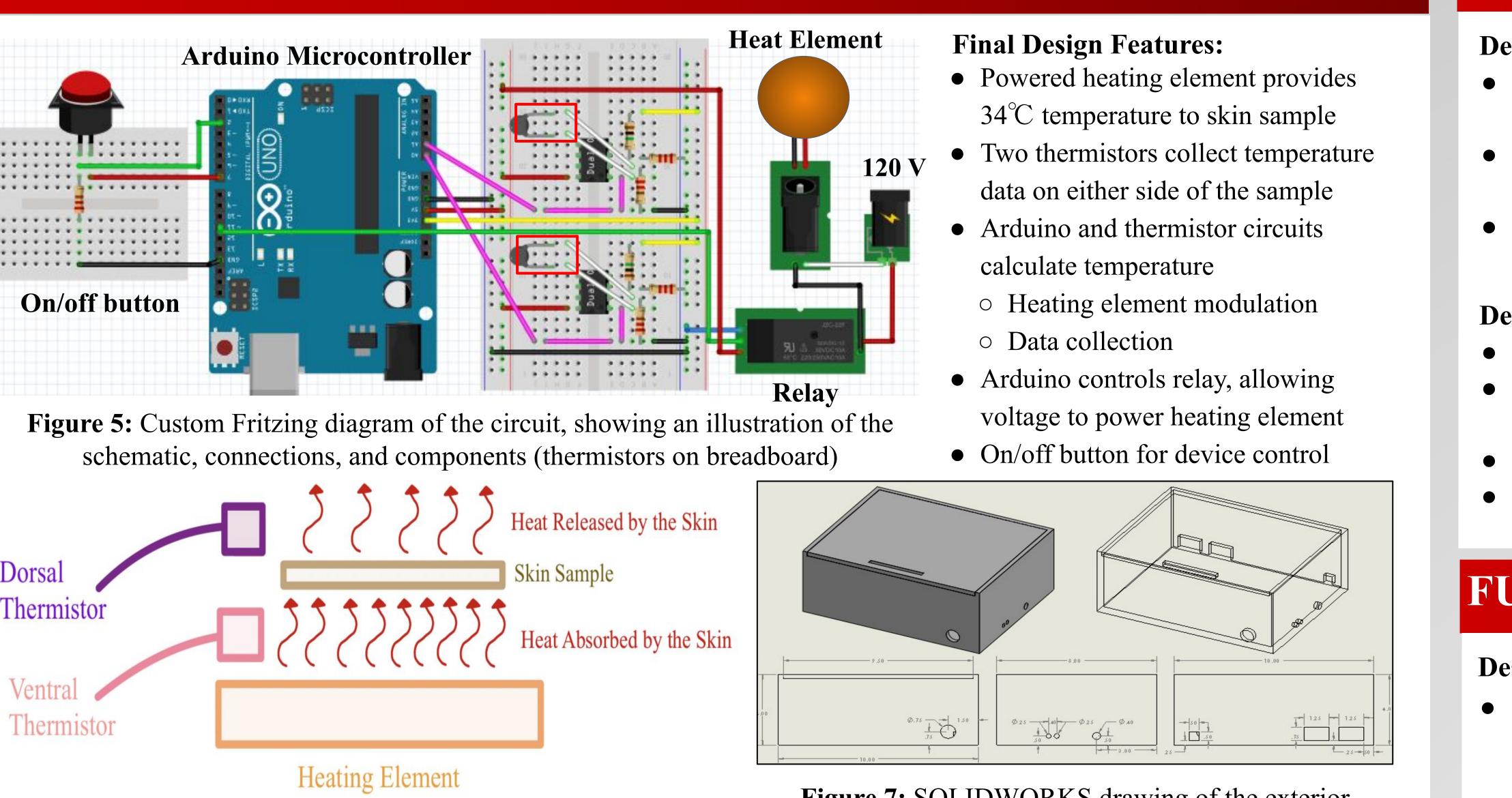


Figure 6: Overall design summary

TESTING & RESULTS

Heating Element

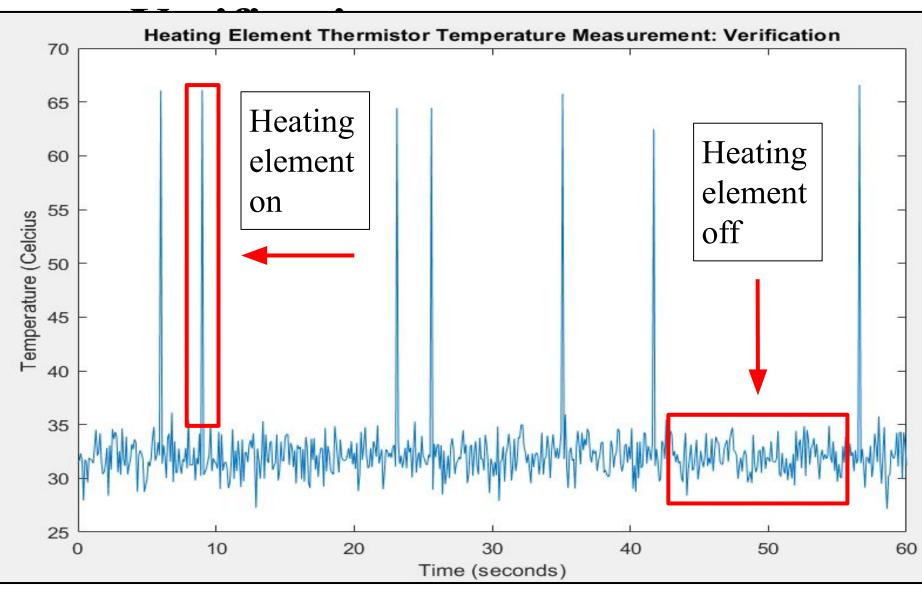


Figure 8: Graph showing the thermistor temperature reading of the heating element over time while running

Skin Temperature Test

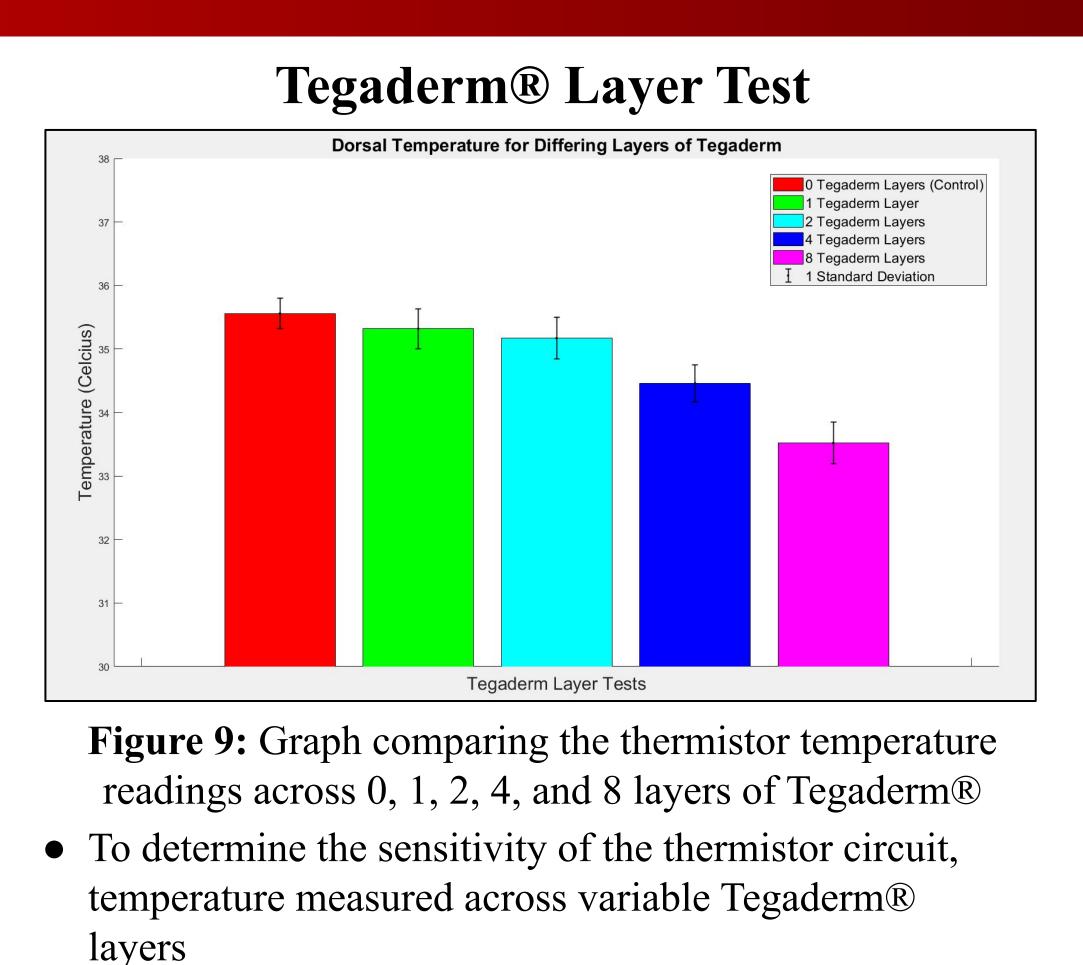
• Skin temperature was measured using the thermistor and infrared thermometer, and a student t-test was conducted

Table 1: Means, standard deviations and p-value for 10

 second temperature readings via thermistor and infrared

	Mean (°C)	Standard Deviation (°C)
Thermistor	34.91	0.3520
Infrared	33.2	0.2938
p value	$1.24\text{E-}7 < \alpha = 0.05$	

box containing the circuit



• A multiple comparison test was performed to evaluate $1.00\text{E-5} < \tilde{a} = 0.01$ p value

- The p-values for both the Skin Temperature Test and Tegaderm[®] Layer Test are below respective α values • Skin Temperature Test null hypothesis of <u>no difference</u>
- between temperature measurement methods; and Tegaderm® Layer Test null hypothesis of <u>no difference</u> in dorsal temperature between layers are both rejected.

Design Drawbacks

- element

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"mp1-t	[2]
"Epide	[3]
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W. Tan	[4]
Mecha	
"Phy	[5]
"Mana	[6]
"Printe	[7]
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DISCUSSION

Design Achievements

• The final device is sufficient in measuring the temperature on the dorsal surface of skin without accounting for evaporative cooling.

• Heating element verification testing showed that the skin sample is supplied with approximately 34°C consistently on the ventral surface.

• Device is adequately sensitive in measuring the temperature through variable layers of Tegaderm® with recognizable difference, as shown in Figure 9.

• Tape is required to ensure thermistor contact with skin sample.

• The heating element heats exceedingly fast, reaching temperatures of 70°C before the sampling frequency of the Arduino allows a response.

• Breadboard connections and inexpensive components possess inaccuracies. • Limited resolution of the Arduino and noise contribute to inconsistencies in temperature measurements, as shown in Figure 8.

FUTURE WORK

Design future work:

• Create a PCB (printed circuit board) of the device's circuit, as shown in Figure 10 • Increase accuracy of connections and decrease footprint

• Incorporate a higher quality heating

• Design a mechanism for applying the thermistors to skin sample and heating element instead of tape (Figure 11)

Testing future work:

• Repeat heating element verification with adjusted resolution and heating element • Test against Thermtest MP-1 device • Perform ergonomics testing with the final design for researcher evaluation

• Ouantify ease of use, other PDS criteria ACKNOWLEDGMENTS

Caroline Alexander Justin Williams • Dr. John Puccinelli

Figure 10: Visualization of an assembled PCB [7]

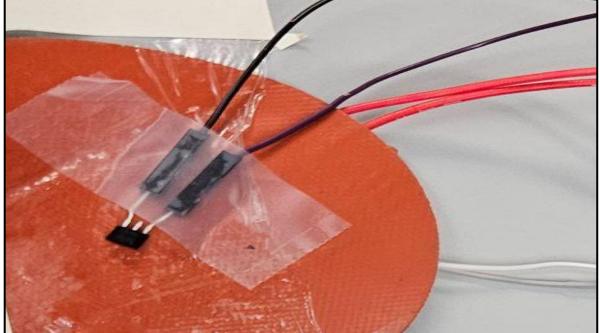


Figure 11: Thermistors taped to Tegaderm[®] and heating element

- UW-Madison MakerSpace
- UW-Madison TEAMLab
- UW-Madison BME Department

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