

Abstract

Myocardial infarctions, commonly known as heart attacks, are responsible for one in four American deaths each year. Ischemia is the lack of oxygen delivery, and is a cause of cardiac cell apoptosis. Heart cells are terminally differentiated, so in the event of mass apoptosis, the heart is severely weakened. Current cardiac research is focused on determining the ideal conditions for fusing mesenchymal stem cells with ischemic heart cells. Combining fine gas control and detection with a microfluidic system will simulate an in vivo environment more closely than previous methods. The end goal of this design is to develop a microfluidic-based hypoxia chamber to facilitate studies involving oxidative stress, ischemia, and reactive oxygen species (ROS)-mediated cellular pathways.

Background and Motivation

- Myocardial infarctions cause one in four American deaths each year [1]
- Cardiomyocytes die within 3-4 hours of oxygen deprivation [2]
 - Terminally differentiated (cannot divide)
 - Seek ideal conditions for differentiation and fusion of mesenchymal stem cells with heart cells
- Commercial hypoxia chamber (Figure 1):
 - Not cost effective [3]
 - Slow equilibration time [4]
 - Unable to establish spatial gradient
 - Inaccurate model of in vivo conditions
 - Limited to gas input

Design Criteria

- Develop microfluidic based hypoxia chamber
- Generate spatial O₂ gradient 21% 0%
- Materials housing cells must be biocompatible
- Channel dimensions $250 750 \mu m \times 250 500 \mu m$ (W x H)
- Function inside cell incubator at 37° C and 5% CO_2

Device Design

- Operates by diffusion of O₂ gas
- O_2 and N_2 gas inputs
- Variable gradient function of pressure input
- Eight longitudinal channels orthogonal to gas inputs (Figure 2) \circ Longitudinal channel dimensions = 31 x 0.75 x 0.25 mm (LxWxH)
 - Regions for cell culture



chamber

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Figure 1: Macro-scale hypoxia

Figure 2: Photomasks for top and bottom layers of master template







Master template production

Polydimethylsiloxane (PDMS) mold

Oxygen Detection

basic solution [NaOH] (Figure 5)

- Solution blue in presence of O_2 (Oxidized)
- Blue (Oxidized form) **H⁺**, 2 e⁻ (CH₃)₂N² $N(CH_3)_2$

Microfluidic Gas Diffusion Platform

Figure 3: At input pressure of 2,500 Pa, O₂ gradient ranges from 1.26 $[mol/m^3]$ to 0.1 $[mol/m^3]$ (COMSOL[®])

Diffusion/Convection $\nabla \bullet (-D_i \nabla c_i) + u \bullet \nabla c_i = R_i$

#)•1,803.57)	•	\bullet $P[Pa]$	
)	R	$\frac{J}{K \bullet mol}$	• <i>T</i> [<i>K</i>]

Spin SU-8 onto silicon wafer Pre-bake cycle (Intervals of 65° and 95° C) Expose photomask covered wafer to UV light to crosslink SU-8 (**Figure 4**) Post-bake cycle (Intervals of 65° and 95° C) Repeat for subsequent feature layers Rinse in SU-8 developing solution to remove non-solidified regions

Pour PDMS onto master template • Place in vacuum until void of bubbles • Bake on hot plate at 80° C for 240 minutes • Separate PDMS from silicon wafer



• Solution colorless in low O₂ concentration (Reduced)









Figure 7: Methylene blue solution saturated



Figure 8: Methylene blue solution saturated with 95% O_2 gas

3 replicates tested at each of the following: 0%, 21%, 95% O_2 concentration for color channel intensity (Figures 6, 7, 8) Color intensity calculated for aggreage and indiviual color channels

Results statistically significant for all channels (Figure 9, Table 1)

Color Channel → RGB -Green

Light Intensity Measurement	P-Value	
RGB	0.0000444*	
Green	0.0000909*	
Red	0.00000195*	
Blue	0.000513*	
*p<0.001		

Table 1: Single Factor ANOVA Results

- Implement ruthenium (fluorescence) based O₂ sensor strips
- Inhibit cross channel diffusion by coating channel interior with

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